Minireview

OCT imaging of rod mitochondrial respiration in vivo

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Impact statement

New clinical imaging biomarkers of photoreceptor mitochondrial function are needed to improve early diagnosis and interventions in order to prevent vision loss in a range of common retinopathies. The focus of this review is on the development and application of an imaging index of mitochondria-evoked changes in subretinal space (SRS) water content during dark and light conditions, an under-appreciated contributor of outer retina health and disease involving pro-survival factors in the interphotoreceptor matrix. Translating the promising OCT results from animal studies to humans will result in improved diagnosis of mitochondria-based threats to sight in aging and disease, and improve the success rate when translating treatments from bench-to-bedside.

Abstract

There remains a need for high spatial resolution imaging indices of mitochondrial respiration in the outer retina that probe normal physiology and measure pathogenic and reversible conditions underlying loss of vision. Mitochondria are involved in a critical, but somewhat underappreciated, support system that maintains the health of the outer retina involving stimulus-evoked changes in subretinal space hydration. The subretinal space hydration light–dark response is important because it controls the distribution of vision-critical interphotoreceptor matrix components, including anti-oxidants, pro-survival factors, ions, and metabolites. The underlying signaling pathway controlling subretinal space water management has been worked out over the past 30 years and involves cGMP/mitochondria respiration/pH/RPE water efflux. This signaling pathway has also been shown to be modified by disease-generating conditions, such as hypoxia or oxidative stress. Here, we review recent advances in MRI and commercially available OCT technologies that can measure stimulusevoked changes in subretinal space water content based on changes in the external limiting membrane-retinal pigment epithelium region. Each step within the above signaling pathway

can also be interrogated with FDA-approved pharmaceuticals. A highlight of these studies is the demonstration of first-in-kind in vivo imaging of mitochondria respiration of any cell in the body. Future examinations of subretinal space hydration are expected to be useful for diagnosing threats to sight in aging and disease, and improving the success rate when translating treatments from bench-to-bedside.

Keywords: Diffusion MRI, optical coherence tomography, mitochondria, photoreceptors

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Introduction

Detection and treatment of sight-threatening retinal disease typically involve imaging structural damage of, for example, the photoreceptors and retinal pigment epithelium (RPE). However, clinical identification of histopathology is often at a stage with irreversible damage and thus at a time when interventions would not restore lost vision. Before morphological manifestation of ocular diseases, there are usually functional/mitochondrial defects in photoreceptors and/or their support system; however, such dysfunction is not usually measured. New functional

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biomarkers are needed to evaluate photoreceptor function and their mitochondrial-based support system that maintain a healthy environment and evaluate treatment efficacy against vision loss. Preferably this will be achieved using instruments already available in clinic and laboratories. The focus of this review is on the development and application of imaging indices of a key aspect of this support system: measuring mitochondria-evoked changes in subretinal space (SRS) water content during dark and light conditions, an under-appreciated contributor of outer retina health and disease.

Current functional indices of cone and rod photoreceptors

Cone and rod function are often evaluated using the electroretinogram (ERG) (both Ganzfeld and multi-focal ERG $[{\rm mfERG}]$ ¹⁻⁷ These methods measure an integrated signal from the entire retina indicating phototransduction and outer retina synaptic transmission. However, their no-tolimited spatial resolution makes lesion detection sensitivity and specificity low.1–7 For example, ERG has not been able to predict loss of visual performance in models of retinal degeneration nor in aging in the absence of overt pathology.^{8,9} In addition, changes in retinal laminae electrical resistance will alter ERG readout confounding any interpretation of the role of mitochondria. To address these shortcomings, new optoretinographic (ORG) methods are being developed that encode light-based changes (thickness or reflectance) in cone and rod photoreceptors with very high spatial and temporal resolution, and are likely insensitive to changes in electrical resistance.¹⁰⁻¹² While much progress has been made in identifying the mechanisms underlying ORG signals, including a report of a mitochondrial contribution, the earliest change appears to reflect electromechanical deformation in individual human cone photoreceptors.^{10–15} It is unclear at present whether the fast ORG response is able to evaluate modifiable prosurvival factors within the photoreceptor-retinal pigment epithelium (RPE) support network.

The photoreceptor support system depends on light–dark changes in SRS hydration

The SRS is the extracellular fluid space between RPE cells and photoreceptors, spanning from the posterior border of the Müller glia (i.e. the external limiting membrane [ELM]) to the apical RPE.¹⁶ This space is relatively isolated by tight junctions at these the two borders. In most mammalian (rod-dominate) retina, the inner and outer segments of rod photoreceptors largely occupy the SRS which contains the interphotoreceptor matrix (IPM) and extracellular fluid.¹⁷⁻²² The IPM is thought to contribute to the essential maintenance and healthy performance of photoreceptor cells by regulating nutrient and retinoid transport, prosurvival/anti-oxidant factors, and ion composition.17,18,23,24 Notably, the IPM has been implicated in neurodegenerative disease.^{18,25}

Somewhat surprisingly, many components of the SRS normally undergo a major shift in their distribution within the IPM between light and dark conditions; abnormal distribution appears to be of pathogenic importance.18,20,24,26 This shift in IPM content dispersal is linked to two other stimulus-induced changes. First, as shown by microelectrode studies, pH outside of rod photoreceptors in the dark decreases (i.e. acidify) in cat retina in vivo.^{27,28} Light-induced extracellular alkalinization near rod photoreceptors was also reported for ex vivo toad and rabbit retinas.29,30 These findings support the large and well established increase in mitochondria respiration in the dark over that in the light which is linked to keeping cGMP channels in the open position.³¹⁻³³ Second, in the dark substantial shrinkage of SRS, volume has been measured in frog and chick retinal preparations ex vivo, and in cat retina in vivo using microelectrodes and an extracellular marker.27,34–38 Intriguingly, blocking RPE ion channels with 4,4′-diisothiocyanostilbene-2,2′-disulfonate (DIDS) inhibited the stimulus-dependent IPM volume change.³⁶ Also, lowering IPM pH alone with carbonic anhydrase inhibitors (i.e. acetazolamide or benzolamide) is sufficient to decrease SRS volume in perfused light-adapted chick retina– RPE-choroid preparation; in-line with this response, acetazolamide is useful for increasing subretinal fluid resorption in patients.³⁹ Further, hypoxia, a diseasegenerating condition that can lower the pH outside of rods, also suppresses light-dark SRS volume changes.^{40,41} Mechanistically, Adijanto et al. showed how lower pH can trigger a reduction in SRS volume.³³ In RPE cells, they found that dark-like increases in $CO₂$ and waste water can acidify the SRS, an event that turned on water removal co-transporters in RPE that caused rapid removal of the acidified SRS water in order to protect rods and cones.33,37,42–48

In summary, the above findings from 1990 to 2009 provide strong support for the following signaling pathway (summarized in Figure 1). In the dark, cGMP levels in the outer segments are relatively higher and ion channels stay open which requires greater mitochondrial respiration resulting in acidification of SRS due to increased $CO₂$ production. In turn, this acidified IPM upregulates water efflux co-transporters in the RPE. As a result, higher RPE fluid transporter activity occurs that overcomes enhanced water production of increased mitochondrial respiration and reduces the SRS water content causing ELM-RPE thickness to shrink (Figure 1(a)). In the light (Figure 1(b)), when cGMP levels in the outer segments are low, ion channels are closed, requiring less energy to maintain circulating current and, therefore, supporting mitochondrial respiration is reduced. Reduced mitochondrial respiration also generates less $CO₂$ byproduct, and pH in the SRS is thus relatively more basic. This pH keeps water efflux cotransporter activity in the RPE low. Although reduced mitochondrial respiration generates less water as another byproduct, down-regulated fluid co-transporters on the RPE lead to accumulation of water in the SRS producing a relatively thicker ELM-RPE compared to that in the dark.

So, is this light-evoked SRS expansion or dark-evoked SRS shrinkage?

The literature largely refers to the above events as a lightevoked expansion of the ELM-RPE.³⁸ This description does not, in our opinion, adequately capture the active mechanism (see Figure 1).³⁸ Our preference is to refer to the above signaling pathway as a dark-evoked thinning of the ELM-RPE in order to focus on the fact that dark actively triggers water removal from the SRS via upregulated pH-sensitive RPE co-transporters; herein, we refer to this as the cGMP \rightarrow

Figure 1. Working model outlining how the SRS volume changes hydration with dark and light conditions. (a) In the dark, cyclic nucleotide-gated ion channels (left most cartoon) are maintained in an open position via availability of cGMP (up arrow), causing increased ion pumping and associated increase (up arrow) in mitochondrial (second cartoon) respiration. In turn, rods produce more waste water (# of droplets) and CO₂ that together lower (down arrow) the pH of the SRS. Water $+CO₂$ make an acidified environment that upregulates water efflux co-transporters (faucet cartoon) on RPE causing a reduction in SRS volume (indicated by smaller font). A smaller SRS volume is measured by a thinner ELM-RPE thickness. (b) In the light, cGMP is hydrolyzed reducing its concentration and causing cyclic nucleotide-gated channels to close, reversing the events in (a) and producing a larger SRS volume than in the dark with a thicker ELM-RPE region. Each step in this signaling pathway has been experimentally demonstrated (see text for details). (A color version of this figure is available in the online journal.)

mitochondria \rightarrow pH \rightarrow RPE water removal signaling pathway.

Measuring light–dark SRS hydration changes in vivo: Diffusion MRI

In 2012, Bissig and Berkowitz non-invasively showed a dark-evoked decrease in the apparent diffusion coefficient (ADC) in SRS region in rats as measured by MRI.⁴⁹ Diffusion MRI has a spatial detection sensitivity of \sim 5 µm and is exquisitely sensitive to changes in water mobility due to changes in cellular barriers and shapes, as shown for a mouse eye (Figure 2(a)).^{50,51} Thus, the light-dark diffusion MRI changes likely reflected the expected darkevoked shrinkage of the SRS volume. Another finding from this study was that water mobility in the SRS region is much higher than in the rest of the retina suggesting a distinct and localized water management system.⁴⁹ Also, light–dark changes in water mobility occurred in the axial direction (in the direction parallel to the rods) and not in the transverse direction.⁴⁹ This was also the first study to indicate light–dark changes in SRS hydration in rats, and subsequently shown in mice.⁵⁰⁻⁵²

In 2015, diffusion MRI also showed light–dark changes in the SRS region in mice (Figures 2(b) and 3).⁵² Further, the diffusion SRS photoresponse was first shown to be phototransduction-dependent because it was absent in GNAT1 knockout mice (Figure 3).⁵² Intriguingly, stimulus-evoked SRS changes were also not seen in diabetic mice but could be recovered 30 min after giving an antioxidant, demonstrating an unexpected sensitivity to oxidative stress (Figure 3). $52,53$ One likely mechanism for this surprising result is that oxidative stress is associated with acidification, a condition expected to inhibit light–dark SRS hydration changes (see above). 54 In support of this notion, in 2016, we presented data showing in vivo that lowering SRS pH alone with acetazolamide given to non-diabetic mice also prevented light–dark SRS changes measured by diffusion MRI (Figure 3).⁵⁵

In summary, these studies from 2012 to 2016 demonstrated that light–dark SRS changes are sizable enough in vivo to generate endogenous contrast that is detectable with imaging. These studies opened the way to considering similar imaging studies in patients using optical coherence tomography, a more clinically accessible technology than MRI.¹⁷⁻²²

OCT studies of light–dark SRS hydration changes in vivo

OCT is commonly used both in clinic and research for providing a non-invasive optical section of the retina. In 2016, Li et al. reported shrinkage of outer retina thickness after dark-adaptation in the same mouse.⁵⁶ To quantitate outer retinal layer thickness changes, outer retina thickness was measured from two clearly distinguishable OCT markers, external limiting membrane (ELM) and basal side of RPE layer. In commonly used C56B/6J mice, 4-6 µm reductions in ELM-RPE thickness were observed on OCT images after over-night dark-adaptation (Figure 4(a)); more recent work finds that the ELM-RPE phenotype in the light can be converted to a thinner dark-like phenotype with a phosphodiesterase 6 inhibitor sildenafil (Figure $4(b)$).^{56,57} Good agreement was noted with light–dark changes in staining of the actin in the IPM as measured histologically.⁵⁶ In addition, the authors noted a novel OCT photoresponse with a strong hyporeflective band between the RPE and photoreceptor-tip layers in the light that was suppressed in the dark; work is on-going to understand how this hyporeflective band and ELM-RPE changes are related.^{56,58}

OCT studies demonstrating mitochondria control of light–dark SRS hydration changes

We then asked if differences in mitochondria respiration could be interrogated based on the ELM-RPE thickness.

Figure 2. Diffusion MRI measures dark-light differences in the SRS volume in vivo. (a) Typical MRI image of a mouse eye (left-most image) indicating that the shape of isotropic water movement (as measured by diffusion MRI) changes from circular/spherical in the absent of barriers (e.g. in the vitreous) to more constrained/oblong in the extracellular fluid surrounding rod photoreceptors. Thus, a decrease in SRS volume is predicted to decrease isotropic water movement as water encounters more barriers. (b) Summary of retinal water mobility (i.e. apparent diffusion coefficient [ADC]) profiles as a function of retinal depth during dark (black, dark lightbulb) and 20 min of -500 lux light (pink, yellow light bulb) for wildtype C57BL/6J mice. A representative OCT image is presented at the top of the graph (after aligning the vitreousretina and retina-choroid boundaries) to provide a guide for assigning a particular ADC value to a particular retinal laminae; indicated are the outer nuclear layer (ONL), external limiting membrane (ELM), inner segments (IS), outer segments (OS), and retinal pigmented epithelium (RPE). Profiles were spatially normalized to whole retinal thickness for each mouse (0% = vitreous/retina border; 100% = retina/choroid border). Data are means ± SEM. Black horizontal line = region with significant differences $(P < 0.05)$ between profiles. This graph highlights (i) that in the light water mobility is greatest in the SRS relative to other parts of the retina, and (ii) that a darkevoked decrease in ADC is localized to the SRS region (e.g. 92–100% retinal depth), as predicted by the signaling pathway in Figure 1 and microelectrode studies in the literature.

Figure 3. Diffusion MRI data supporting signaling pathway factors in Figure 1 that contribute to the SRS volume changes in light and dark. Summary of paired data (filled $=$ dark, open $=$ light) of wildtype (WT) mice) showing a nice reduction in ADC in the dark, mice without the phototransduction protein transducing $(GNAT1^{-/-}$ mice) do not show a light-dark difference, acidified SRS by acetazolamide (AZM) do not show a light–dark difference, and vehicle or an antioxidant (α -lipoic acid, LPA) treated two-month diabetic mice (STZ, STZ + LPA, respectively) show the presence of oxidative stress (which can acidify neurons). Red horizontal line, $P < 0.05$.

In 2018, we compared two mouse strains with different mitochondrial respiration efficacies (lower C57BL/6J vs. higher 129S6/SvEvTac).⁵⁸ Mitochondrial respiration efficacy refers to the amount of oxygen needed to produce ATP; mice with less efficient mitochondria (e.g. C57BL/6J) are vulnerable to retinal degeneration involving, for example, oxidative stress.59,60 Dark-stimulated outer retina layer water content was determined by proton density MRI, structure and thickness by ultrahigh-resolution OCT, and water mobility by diffusion MRI.⁵⁸ In C57BL/6J mice, dark adaptation triggered a decrease in water content of outer retina in vivo together with a decrease in the ELM-RPE thickness, and in water mobility (Figure 5(a)). In contrast, dark did not change SRS hydration or decrease water mobility in the 129S6/SvEvTac mice; a significant but relatively smaller decrease in ELM-RPE thickness was noted (Figure 5(a)).⁵⁸ In other words, a large light-dark ELM-RPE thickness change was linked to less efficient mitochondrial respiration. These studies raise the possibility of the size of the light–dark ELM-RPE thickness change may be a useful mitochondrial injury biomarker.

Next, we took advantage of mitochondrial uncouplers, such as 2,4-dinitrophenol (DNP), which shuttle protons across the mitochondrial inner membrane thus disrupting the mitochondrial proton gradient that is used to generate ATP, to stimulate metabolism if sufficient reserve capacity is available. 61 In the light, DNP produced dark-like ELM-RPE thickness in both C57BL/6J and 129S6/SvEvTac mice, with a larger thinning in C57BL/6J consistent with its relatively less efficient mitochondria respiration (Figure 5 (b)). $58,59,61$ In the dark, when photoreceptor mitochondria activity is high, DNP had no significant effect on ELM-RPE thickness in dark-adapted C57BL/6J mice (implying little mitochondrial reserves) but did cause thinning in

Figure 4. Modifiers of the ELM-RPE thickness. (a) Light vs. dark: Zoomed-in region of the ELM-RPE in a representative mouse that was exposed to either 5 h of lab light or was overnight dark adapted; brackets provide a visual guide to highlight dark-evoked shrinkage of the ELM-RPE thickness. Quantitation of this light-dark change is provided in the first two bar graphs in (b) (also in Figure 5). (b) Pharmacology: Bar graph summary comparing dark (D, black bar) and light (L, white bar) adapted ELM-RPE thicknesses to a light-adapted mouse given the phosphodiesterase 6 inhibitor sildenafil (green bar) 1 h prior to examination. Data are means ± 95% confidence intervals; data for each mouse also shown as individual points. Black horizontal lines = significant differences between groups ($P < 0.05$). (A color version of this figure is available in the online journal.)

Figure 5. Evidence that mitochondria drives changes in ELM-RPE thickness. (a) Light vs. dark: Summary of outer retina thickness, measured from OCT images in light (L) and dark (D) for mice with relatively inefficient mitochondria respiration (C57BL/6J [B6]) and with relatively more efficient mitochondrial respiration (129S6/SvEvTac [S6]). This means that in the light, S6 mice have a lower basal level of mitochondria activity than B6 mice resulting in lower waste water production and thus shorter ELM-RPE thickness and smaller light–dark difference. (b) Pharmacology: Paired differences (before-after DNP) are presented to account for changes within mice. Individual data points (= number of eyes examined; one eye per mouse) represent the replicate average for each mouse to illustrate animal-to-animal variation. Specific stimulation of mitochondria with a protonophore again resulted smaller ELM-RPE in light-adapted S6 mice compared to that in B6 mice, in agreement with the light-differences in (a). In all graphs, horizontal range bar indicates the region with significant differences (P < 0.05); error bars represent 95% confidence intervals.

129S6/SvEvTac mice (consistent with residual mitochondrial reserves) (data not shown). 61 Work is on-going to test the prediction that acidifying the SRS with systemic acetazolamide will produce a dark-like ELM-RPE phenotype in light-adapted mice.

Can OCT measure oxidative stress in subretinal space?

Subretinal oxidative stress is thought to be a pathogenic factor for many blinding diseases, such as age-related macular degeneration, diabetic retinopathy, and retinitis pigmentosa, but until recently was not measured in vivo using OCT.⁶²⁻⁶⁶ As noted above, MRI measured an

impact of oxidative stress on SRS water mobility suggesting that excessive free radical production prevented the expansion of the ELM-RPE thickness in light-adapted mice. This effect is consistent with the expected acidification by oxidative stress that would be expected to inhibit light–dark SRS hydration changes (see above).^{54,67,68} Thus, we asked if OCT could also detect oxidative stress in the SRS based on anti-oxidant recovery of absent light/dark ELM-RPE changes, as described in the previous section. Using a pharmacologically induced oxidative stress model,⁶⁸ we demonstrated that light–dark differences in outer retina on OCT images are eliminated in the presence of oxidative stress.⁶⁷

After acute administration of antioxidants (i.e. a "quench" of oxidative stress), ELM-RPE thickness is restored to control levels. Therefore, comparing light/dark OCT responses in outer retina with and without antioxidants "quench" demonstrates a new functionality for OCT: measuring oxidative stress. We call this approach QUEch-assiSTed (QUEST) OCT. As OCT systems are commonly available in both clinic and laboratories, QUEST-OCT technique is expected to provide a useful non-invasive and convenient index of oxidative stress in the retina for diagnosis and intervention.

Future opportunities and challenges

As discussed above, to study mitochondria in photoreceptors, extended periods of dark vs. light conditions are usually used to produce SRS hydration changes as measured by OCT. However, it is unclear if these prolonged light/ dark conditions are suited for routine clinical use. One potential solution to this problem is to take advantage of FDA-approved pharmaceuticals to more quickly interrogate mitochondrial respiration. In this case, two OCT images can be collected, before (i.e. light adapted) and 1 h after inducing a dark-like condition, either with a low dose of mitochondrial uncoupler or phosphodiesterase 6 inhibitor (e.g. sildenafil, Figure 4(b)).

Shorter light exposure protocols (i.e. ORG) might also be useful to speed up probing of the signaling pathway in Figure 1 but more work is needed to unravel the mechanism underlying the ORG responses. In 2017, Zhang et al. reported changes on OCT images of C57BL/6J mice elicited by a brief flashes instead of hours long dark vs. light conditions.⁶⁹ With this faster light exposure protocol, they saw a change in IS to RPE (IS-RPE) length with the thickness in light being about $2 \mu m$ greater than in the dark and was observed using a non-commercial OCT system. Much smaller light–dark changes in outer retina thickness have been made in human eyes using phase-detection of small optical length changes, submicron light–induced elongation of both rod and cone photoreceptors has been reported.10,70,71 However, whether these changes directly interrogate photoreceptor function or the photoreceptor support system is currently an open question because the time scales are so different. In addition, a fast (millisecond) but smaller magnitude of photoreceptor shrinking was also reported.¹² Based on optical changes of cultured neurons in response to electrical firing, 72 it has been postulated that these light-stimulus-induced changes reflect optical responses to both electrical and osmotic changes with induced phototransduction.⁷³ It is hoped that next generation commercial OCT's will be able to address the smaller light–dark difference associated with short light stimuli in order to improve the detection sensitivity/dynamic range to disease and treatment efficacy. In any event, more work is needed to determine if the underlying mechanism (i.e. $cGMP \rightarrow mitochondria \rightarrow pH \rightarrow RPE water removal signal$ ing pathway) also explains the IS-RPE changes to brief flashes.

As OCT continues to be considered for studying photoreceptor cell biology in addition to structure, careful attention is needed to variables that had not been previously

considered. For example, as shown above, genetic differences in mitochondrial respiration can influence the light– dark ELM-RPE outcomes.58,67 This problem can be addressed by using each subject as their own control in a paired design. It has also been noted that light–dark ELM-RPE thickness showed diurnal variations.⁷⁴ Differences in photoresponses as a function of sex is also possible.

Another key parameter is the duration of dark and light exposure times. Microelectrode studies in excised retina and in vivo investigated changes from dark adaptation after 1–5 min of light. $34,37$ The first diffusion MRI study examined SRS changes following 2–4 min light dark cycles.⁴⁹ In the next study, the diffusion profiles across the retina were compared at 5 and 20 min of light exposure in mice.⁵² The light dark difference was noted at both time points but was substantially larger at 20 min.⁵² The kinetics of light/dark changes in ELM-RPE thickness was further investigated with OCT in a study by Li $et al.⁵⁶$ Compared with \sim 6 μ m changes in ELM-RPE thickness for fully lightadapted (>5 h exposure to room light) and overnight darkadapted mice, 15 min and 2-h light exposure induced elongation of about 2 and $4 \mu m$ in ELM-RPE thickness.⁵⁶ Conversely, 15 min and 2-h dark-adaptation produced shortening to nearly the same extent in ELM-RPE thickness.⁵⁶ In humans, using a 30-min dark adaptation time and bleaching rhodopsin to different extents over several minutes showed a maximum change in ELM-RPE of about $1.5 \,\mu m$ that depended on the bleaching extent.¹¹ Overall, it is clear that the size of the light–dark difference in SRS volume is a function of the light exposure period and dark adaptation period. Together these considerations highlight the need to standardize these periods to facilitate clinical acceptance of the light–dark SRS index and to avoid confounding interpretation of the results between groups.

Conclusions

In this review, we described how OCT can measure mitochondria respiration in vivo for use in diagnosis and intervention based on measuring the photoreceptor-retinal pigment epithelium (RPE) support network signaling pathway that controls modifiable pro-survival factors within the SRS. Our results raise the possibility of measuring mitochondrial respiration in patients using FDA-approved pharmaceuticals.⁷⁵ Overcoming the challenges of performing similar experiments in the clinic will provide a powerful new way to diagnose threats to sight in aging and disease, and improve the success rate when translating treatments from bench-to-bedside.

AUTHORS' CONTRIBUTIONS

All authors participated in the design, interpretation of the studies and review of the manuscript. Both BAB and HQ contributed to the writing of the manuscript.

DECLARATION OF CONFLICTING INTERESTS

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